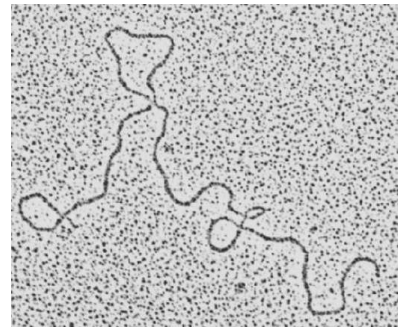
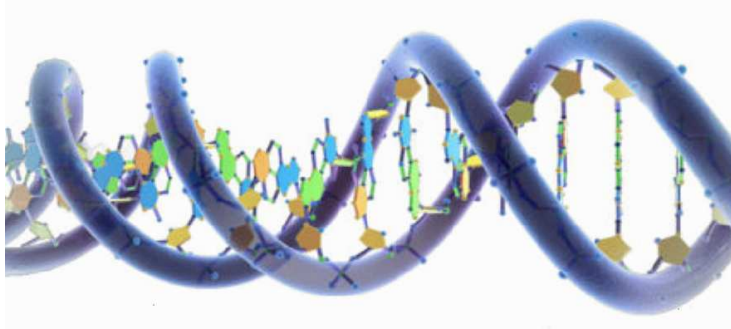


# **Predicting local geometric properties of DNA from hydrodynamic diffusion data**

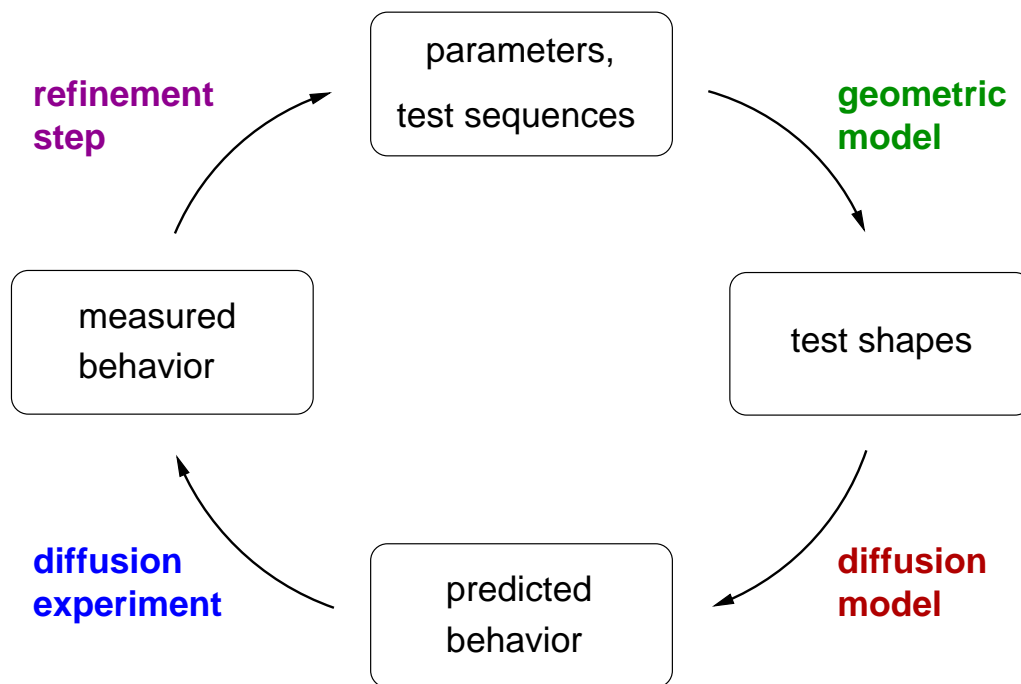
O. Gonzalez, J. Li  
Department of Mathematics  
University of Texas, Austin

# Introduction

**Goal:** To obtain improved estimates of the material parameters that describe sequence-dependent shape of DNA.



**Approach:** Refine parameters through hydrodynamic diffusion modeling and experiments.



# Outline

**Geometric model**

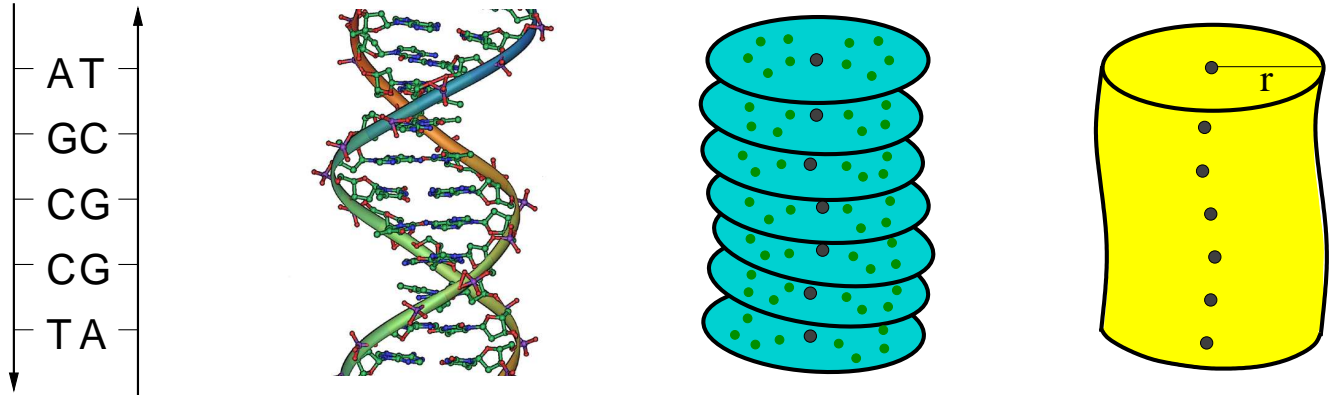
**Diffusion model**

**Application**

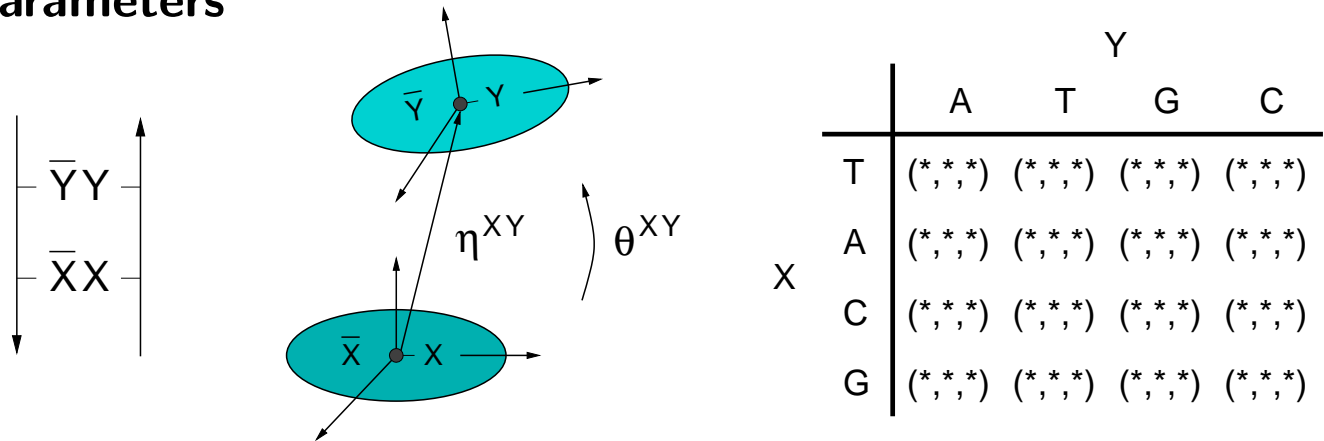
**Results**

# Geometric model of DNA

## Definition



## Parameters



$\eta^{XY}$  = relative displacement for dimer step XY.

$\theta^{XY}$  = relative rotation for dimer step XY.

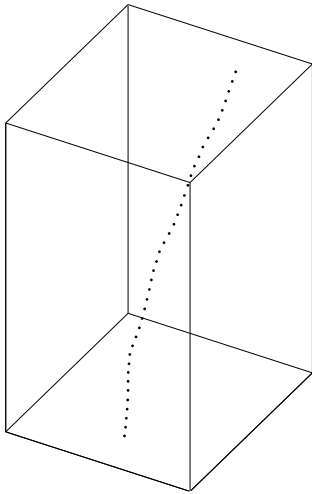
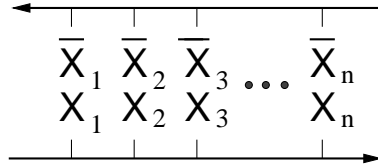
$r$  = radius of tubular surface.

$$\eta = \{\eta^{XY}\} \in \mathbf{R}^{26}, \quad \theta = \{\theta^{XY}\} \in \mathbf{R}^{26}, \quad r \in \mathbf{R}.$$

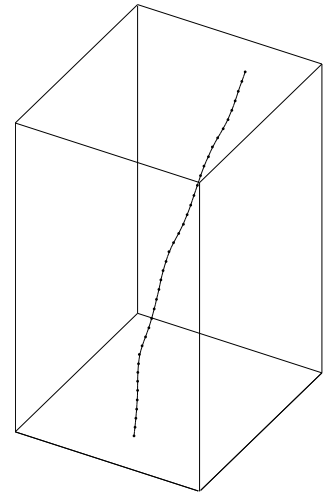
# Geometric model of DNA

## Construction

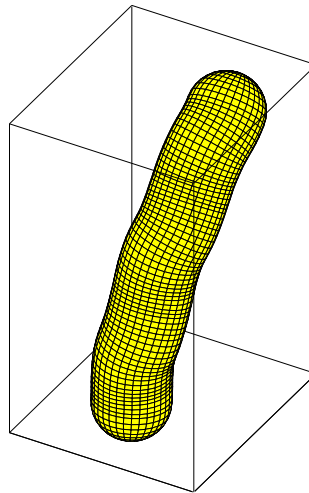
$$S = X_1 X_2 \cdots X_n$$



Reference points  $q_a(S, \eta, \theta)$ .



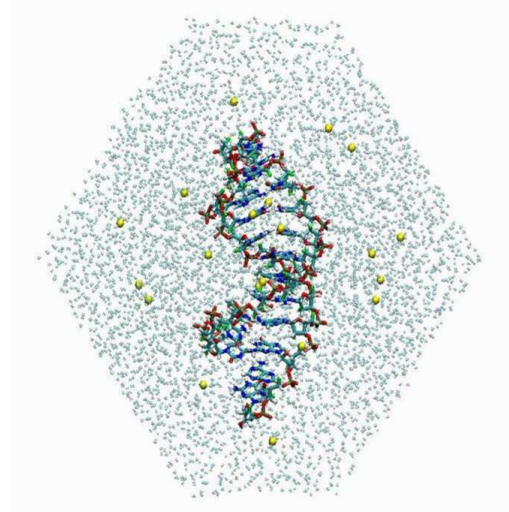
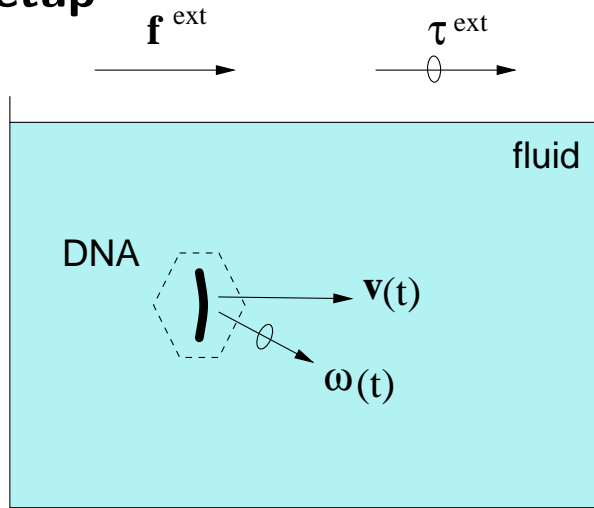
Axial curve  $\gamma(S, \eta, \theta)$ .



Tubular surface  $\Gamma(S, \eta, \theta, r)$ .  
(assumed rigid)

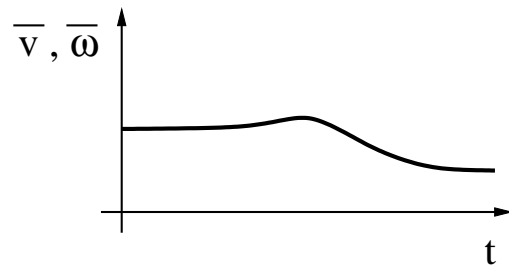
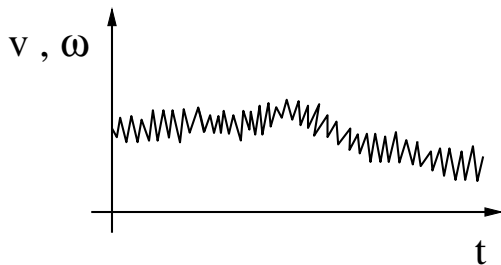
# Diffusion model: single molecule drift dynamics

## Setup



## Drift velocities

$$\bar{v}(t), \bar{\omega}(t) = \frac{1}{T} \int_t^{t+T} v(s), \omega(s) ds. \quad T = \text{window size.}$$

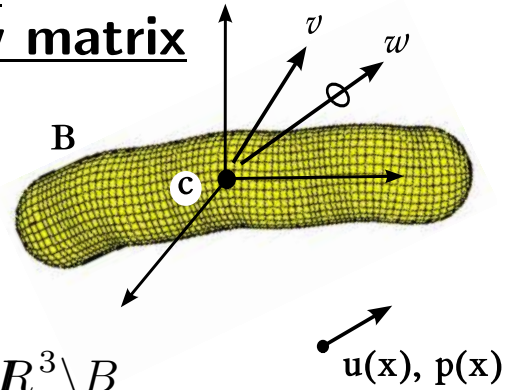


## Governing equation

$$\begin{bmatrix} \bar{v} \\ \bar{\omega} \end{bmatrix} = M \begin{bmatrix} f \\ \tau \end{bmatrix}^{\text{ext}}.$$

$M \in \mathbf{R}^{6 \times 6}$  Stokes mobility matrix  
determined by shape of DNA molecule.

## Diffusion model: single molecule mobility matrix



### Stokes equations

$$\begin{aligned}
 \mu \Delta \bar{u} &= \nabla \bar{p} && \text{in } R^3 \setminus B \\
 \nabla \cdot \bar{u} &= 0 && \text{in } R^3 \setminus B \\
 \bar{u} &= \bar{U}[\bar{v}, \bar{w}] && \text{on } \partial B \\
 \bar{u}, \bar{p} &\rightarrow 0 && \text{as } |x| \rightarrow \infty.
 \end{aligned}$$

### BCs, loads

$$\bar{U}[\bar{v}, \bar{w}] = \bar{v} + \bar{w} \times (x - c)$$

$$\bar{\sigma}_{ij}[\bar{u}, \bar{p}] = -\bar{p} \delta_{ij} + \mu \left( \frac{\partial \bar{u}_i}{\partial x_j} + \frac{\partial \bar{u}_j}{\partial x_i} \right)$$

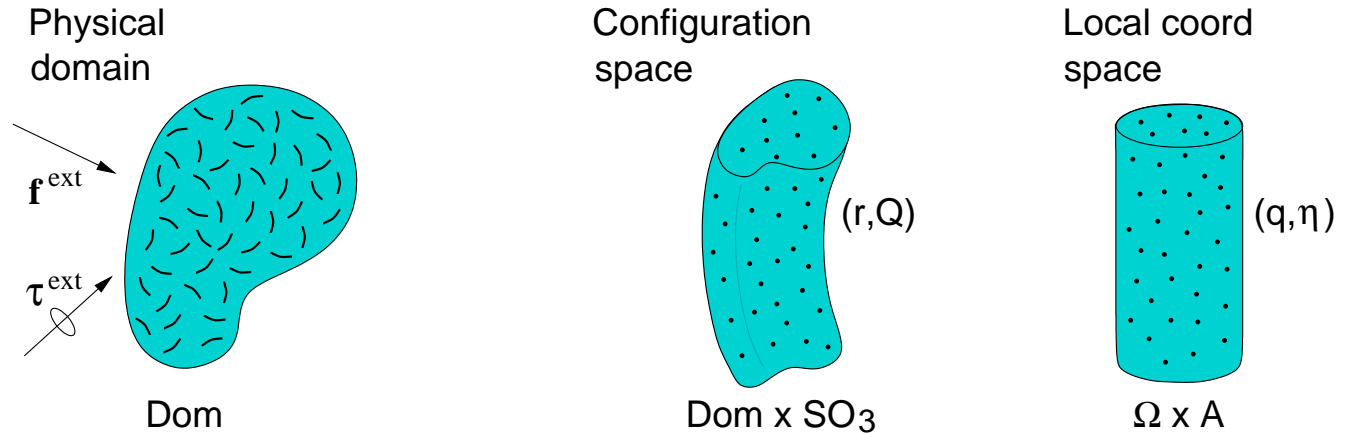
$$\bar{f}[\bar{\sigma}] = \int_{\partial B} \bar{\sigma} n \, dA, \quad \bar{\tau}[\bar{\sigma}] = \int_{\partial B} (x - c) \times \bar{\sigma} n \, dA.$$

### Hydrodynamic matrices

$$\begin{bmatrix} \bar{f} \\ \bar{\tau} \end{bmatrix} = - \underbrace{\begin{bmatrix} L_1 & L_3 \\ L_2 & L_4 \end{bmatrix}}_L \begin{bmatrix} \bar{v} \\ \bar{w} \end{bmatrix}, \quad \begin{bmatrix} \bar{v} \\ \bar{w} \end{bmatrix} = - \underbrace{\begin{bmatrix} M_1 & M_3 \\ M_2 & M_4 \end{bmatrix}}_M \begin{bmatrix} \bar{f} \\ \bar{\tau} \end{bmatrix}.$$

# Diffusion model: collective drift dynamics

## Setup



$\sigma$  = DNA concentration in config space.

$h^{\text{ext}} = (f, \tau)^{\text{ext}}$  = external loads.  $M$  = Stokes mobility matrix.

## Governing equation

$$\begin{aligned}
 \sigma_t + g^{-1} \nabla \cdot (gJ) &= 0 & \text{in } \Omega \times A, & \quad t > 0 \\
 J \cdot n &= 0 & \text{on } (\partial\Omega) \times A, & \quad t \geq 0 \\
 J \cdot n &\text{ periodic} & \text{on } \Omega \times (\partial A), & \quad t \geq 0 \\
 \sigma &= \sigma_0 & \text{in } \Omega \times A, & \quad t = 0.
 \end{aligned}$$

$$J = -D \nabla \sigma + \sigma C h^{\text{ext}}, \quad D = \beta b M b^T, \quad C = b M c.$$

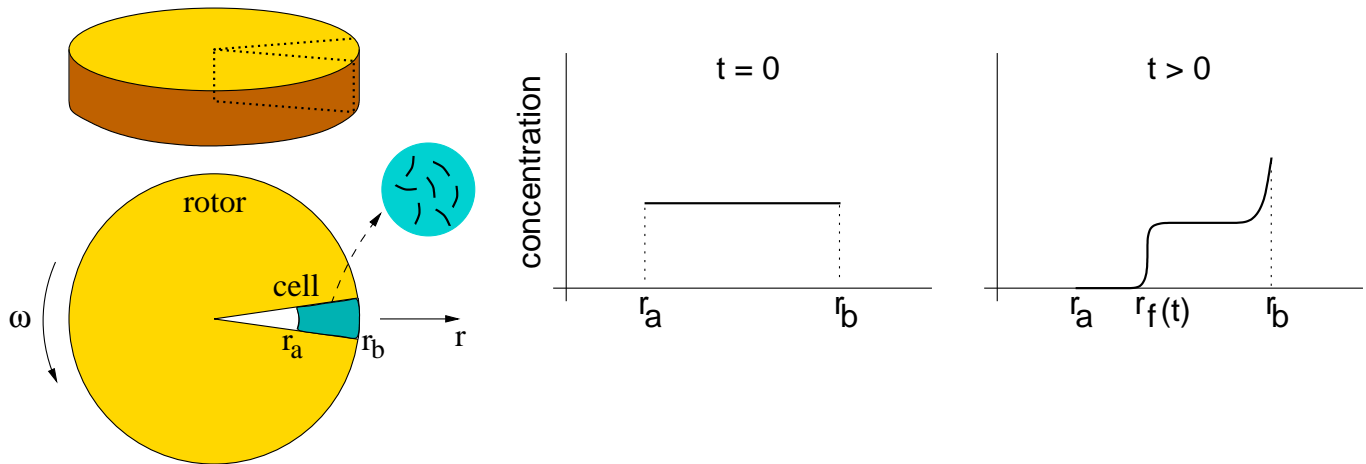
$\beta$  = Boltzmann factor.  $g, b, c$  = geometric factors.

$D, C \in \mathbb{R}^{6 \times 6}$  local diffusion, convection matrices determined by shape of DNA molecule.



## Diffusion model: example experiment

### Ultracentrifuge



Governing eq (dimless).

$$\sigma_t = g^{-1} \nabla \cdot \left[ gD\left(\frac{1}{\varepsilon}\right) \nabla \sigma - g\sigma C\left(\frac{1}{\varepsilon}\right) h^{\text{ext}} \right] \quad \text{in } \Omega \times A.$$

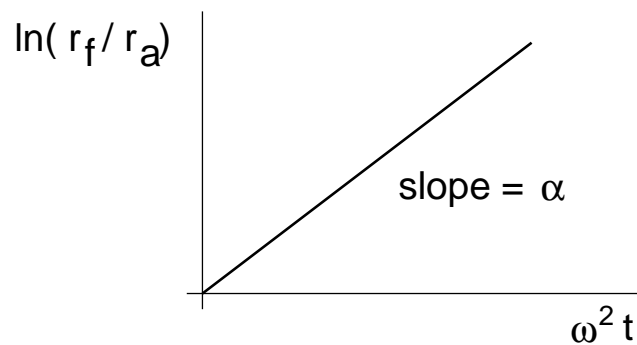
$$\varepsilon \ll 1.$$

Leading-order approx.

$$\frac{\partial \rho}{\partial t} = \frac{1}{r} \frac{\partial}{\partial r} \left[ \kappa r \frac{\partial \rho}{\partial r} - \alpha \omega^2 r^2 \rho \right] \quad \text{in } [r_a, r_b].$$

$$\kappa = f(D), \quad \alpha = \hat{f}(C).$$

Result.



## Diffusion model: summary

- Different diffusion experiments can measure different components of  $D, C \in \mathbf{R}^{6 \times 6}$ , or equivalently,  $M \in \mathbf{R}^{6 \times 6}$ .
- A typical measurable quantity is the translational diffusion coefficient

$$D_t = \frac{\beta}{3} \text{tr}(M_1) \quad \text{where} \quad M = \begin{bmatrix} M_1 & M_3 \\ M_2 & M_4 \end{bmatrix}.$$

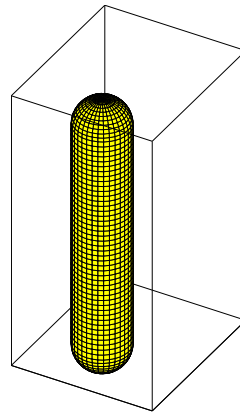
- $M$  and  $D_t$  can be predicted by solving Stokes flow equations around given molecular geometry.

## Application

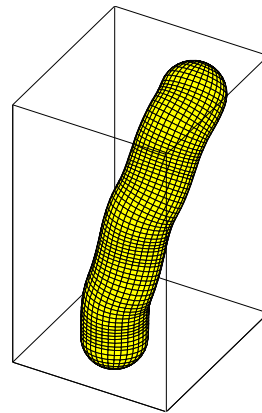
**Given:** Measured values of  $D_t$  on sequences of different length.

**Find:** Radius  $r$  of (hydrated) DNA using two different geometrical models:

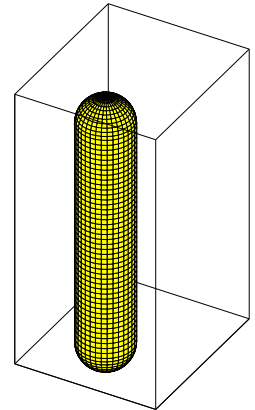
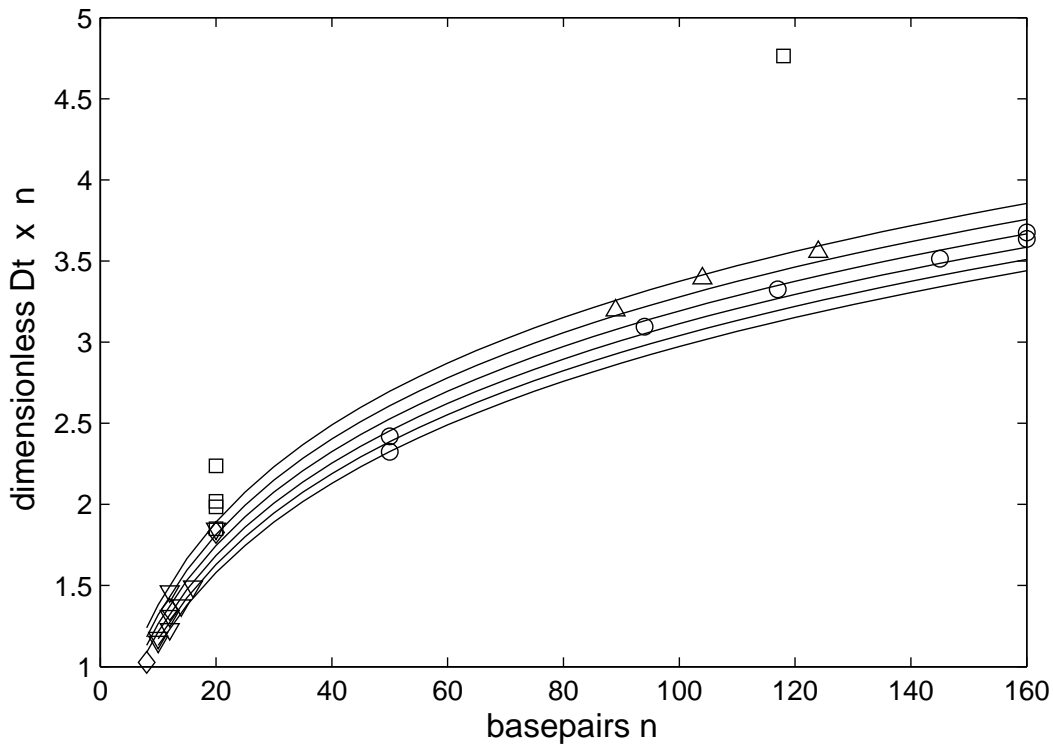
Idealized (straight) model.



Sequence-dependent model.

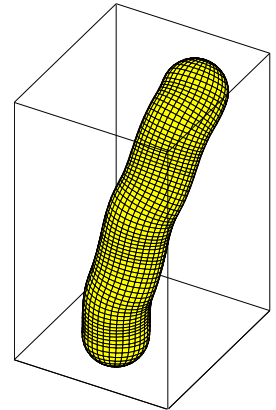
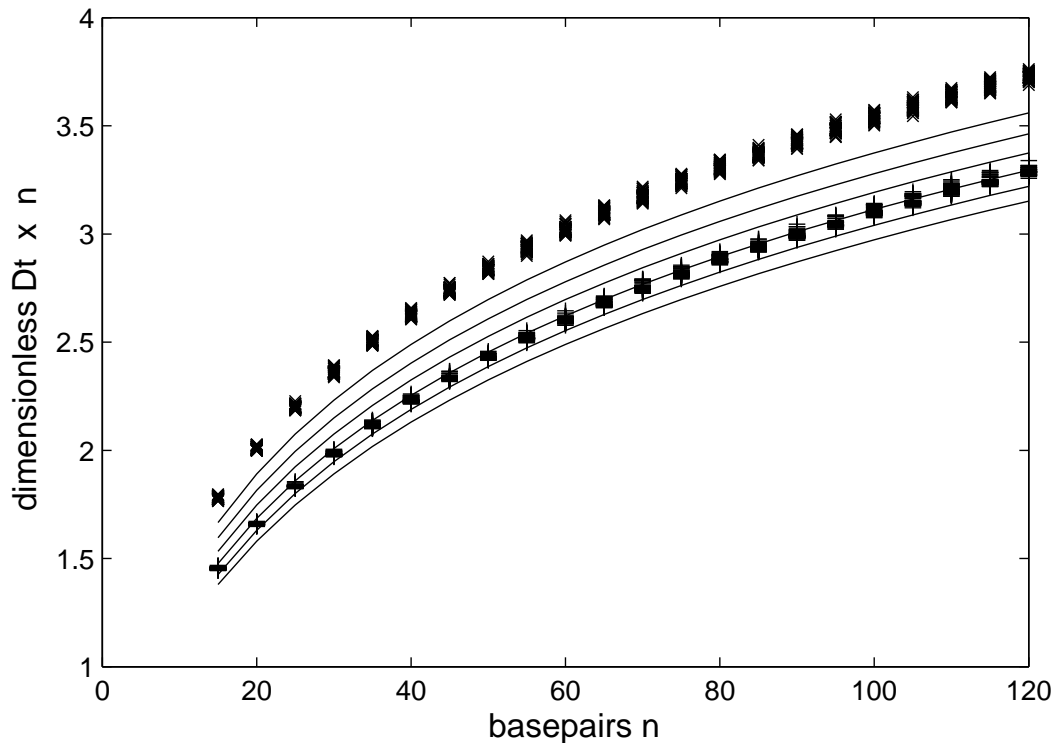


## Results for idealized model: Diffusion coefficient vs length



- Symbols: experiments (ultracentrifuge, light scattering, electrophoresis).
- Curves: numerics  $w/r = 10, 11, \dots, 15 \text{ \AA}$  (top to bottom).
- Results predict DNA radius of  $r = 10 - 15 \text{ \AA}$ .

## Results for sequence-dependent model: Diffusion coefficient vs length



- Curves: straight tube  $w/r = 10, 11, \dots, 15$  Å (top to bottom).
- Crosses: random sequences of prescribed lengths  $w/r = 10$  Å.
- Pluses: random sequences of prescribed lengths  $w/r = 15$  Å.
- Results show systematic offset.
- Results now predict DNA radius of  $r = 12 - 17$  Å.

## Closing remarks

- Simplest model of sequence-dependent DNA geometry involves many parameters ( $\eta \in \mathbf{R}^{26}, \theta \in \mathbf{R}^{26}, r \in \mathbf{R}$ ).
- Estimates for all parameters exist, but there is little consensus.
- Hydrodynamic modeling offers interesting approach to validate/refine parameters.
- Successful realization of approach poses many challenges.

Support

NSF